

AN OVERVIEW OF OCULAR DRUG DELIVERY

***Arnab Majumder, Dr. Falguni Patra and Dr. Beduin Mahanti**

Department of Pharmaceutics, School of Pharmacy, Techno India University, Salt Lake City, EM-4/1, Sector-V, Kolkata-700091, West Bengal, Kolkata, India.

Corresponding Author: Arnab Majumder

Department of Pharmaceutics, School of Pharmacy, Techno India University, Salt Lake City, EM-4/1, Sector-V, Kolkata-700091, West Bengal, Kolkata, India.

Article Received on 22/04/2021

Article Revised on 12/05/2021

Article Accepted on 02/06/2021

ABSTRACT

The major challenge featured by today's apothecary and formulation man of science is ocular drug delivery. Topical eye drop is that the most convenient and patient compliant route of drug administration, particularly for the treatment of anterior section diseases. Also, therapeutic drug levels aren't maintained for extended length in target tissues. Within the past 20 years, ocular drug delivery analysis accelerated advanced towards developing a unique, safe and patient compliant formulation and drug delivery techniques, anterior phase drug delivery advances are witnessed by modulation of standard topical solutions with permeation and viscosity enhancers. The most commonly utilized conventional preparations of ophthalmic dosage forms are the solutions, suspensions and ointments which are relatively inefficient as therapeutic systems. By using prolonged drug delivery, the duration of drug action can be remarkably prolonged and also the frequency of drug administration can be reduced. Such a drug delivery can be achieved by designing formulations such as contact lens, microneedles, nanosuspension, nanoparticles, liposomes, dendrimers, nanomicelles which can act as efficient ocular drug delivery system.

KEYWORDS: Anatomy of Eye, Liposomes, Conventional drug delivery, Nanotechnology based drug delivery.

INTRODUCTION

Drug delivery to the attention has been one amongst the foremost difficult tasks to pharmaceutical scientists. The distinctive anatomy and physiology of the attention renders it a extremely protected organ, and also the distinctive structure restricts drug entry at the target web site of action. Drug delivery to the attention may be typically classified into anterior and posterior segments. standard delivery systems, together with eye drops, suspensions, and ointments, can't be thought of optimal; but, quite ninetieth of the marketed ophthalmic formulations indicated for the treatment of debilitating vision-threatening ophthalmic disorders are within the type of eye drops. These formulations primarily target diseases of the attention (anterior segment). Most locally instilled medication don't supply adequate bioavailability because of the wash of the medication from the attention by numerous mechanisms (lacrimation, tear dilution, and tear turnover). additionally, the human tissue layer composed of epithelial tissue, substantia propria, and epithelium hinders drug entry; consequently, but five-hitter of administered drug enters the attention. Alternative approaches are ceaselessly wanted to facilitate vital drug absorption into the attention. Currently, the treatment of disorders of the rear of the attention (posterior segment) still remains a formidable task for the ocular pharmacologists and physicians. The

tight junctions of blood-retinal barrier (BRB) limit the entry of systemically administered medication into the membrane. High vitreal drug concentrations are needed for the treatment of posterior section diseases. this will be accomplished solely with native administration (intravitreal [IVT] injections/implants and periocular injections). Periocular injections are related to fairly high patient compliance relative to IVT injections. nonetheless, structural variations of every layer of ocular tissue will create a big barrier upon drug administration by any route (i.e., topical, systemic, and periocular). To date, exceptional changes are ascertained within the field of ophthalmic drug delivery.

The EYE (Anatomy): The eye is an isolated, extremely complicated, and specialised organ for photoreception. A fancy anatomy and physiology render it an extremely protected organ.^[1] Generally, the attention is divided into 2 segments: anterior and posterior. The anterior section of the attention consists of tissue layer, mucous membrane, iris, tissue layer, liquid body substance, and lens, whereas the posterior section includes sclerotic coat, choroid, retina, and vitreous humor. The front a {part of} the attention is certain by a clear tissue layer and a second part of the sclerotic coat. The tissue layer and sclerotic coat be a part of along through the complex body part. Tissue layer is empty of blood vessels and

receives nourishment and atomic number 8 offers from the liquid body substance and tear film, whereas the tissue layer outer boundary receives nourishment from the limbal capillaries. The human tissue layer measures around twelve millimeters in diameter and 520 μm in thickness. It's composed of six layers: the Epithelium, Bowman's membrane, stroma, Dua's layer, Descemet's membrane, and epithelium.^[2]

- **Epithelium:** The tissue layer animal tissue may be a stratified, squamous, nonkeratinized layer around fifty fifty in thickness. It is AN outer protecting barrier comprising 5 to 6 cell layers, as well as 2 to 3 layers of planate superficial cells, wing cells, and one layer of columnar basal cells separated by a 10- to 20-nm living thing house. Desmosome-attached cells will communicate by gap junctions through that tiny molecules permeate. The superficial somatic cell layers area unit sealed by tight junctions known as zonulae occludent that stop the permeation of compounds with low lipophilicity across the tissue layer. Thus, the tissue layer animal tissue may be a rate-limiting barrier and hinders the permeation of hydrophilic medication and macromolecules.

- **Bowman's membrane:** This one-celled skinny basement layer is created from scleroprotein fibrils. It's not thought-about as a rate-limiting barrier.

- **Stroma:** Constituting regarding ninetieth of the tissue layer, this layer is abundant in hydrous albuminoid. Thanks to its deliquescent nature, the stroma offers minimal or low resistance to diffusion of extremely deliquescent medication.

- **Dua's layer:** it's a new known, well-defined, acellular, sturdy layer within the pre-Descemet's tissue layer. Its practical role is however to be determined.^[3]

- **Descemet's membrane:** it's a skinny consistent layer sandwiched between the stroma and also the epithelial tissue.

- **Endothelium:** it's a single-layered squamous animal tissue posterior to the tissue layer surface. The stroma and Descemet's membrane cowl the inner epithelium cells, that contain macula adherents. The epithelium cells don't act as a barrier to permeating molecules because of lack of tight junctions.

Conjunctiva may be a vascularized membrane lining the inner surface of eye- lids and also the anterior surface of sclerotic coat up to the body structure. It facilitates lubrication within the eye by generating mucous secretion and helps with tear film adhesion. It offers less resistance to drug permeation relative to tissue layer. Iris, the foremost anterior portion of the complex body part tract, is that the pigmented portion of the attention consisting of pigmented animal tissue cells and circular muscles (constrictor iridial muscle muscles). The gap within the middle of the iris is named the pupil. The iris muscle and dilator muscles aid in standardisation the pupil size, that regulates the entry of sunshine into the attention. The tissue layer, a doughnut-shaped muscle connected to the iris, is made by ciliary muscles and also the ciliary processes. The body fluid, a fluid gift within the anterior section, is secreted by the ciliary processes into the posterior section at the speed of 2 to 2.5 μL/min. It provides most nutrition and atomic number 8 to avascular tissues (lens and cornea). It flows incessantly from the posterior to the anterior through the pupil and leaves the attention via trabeculate meshing and Schlemm's canal. Such continuous flow maintains the pressure (IOP). The lens may be a crystalline and versatile structure fogbound during a capsule. It's suspended from the ciliary muscles by terribly skinny fibres referred to as the zonules. It's important for vision and offers protection to the tissue layer from actinic ray in conjunction with ciliary muscles.

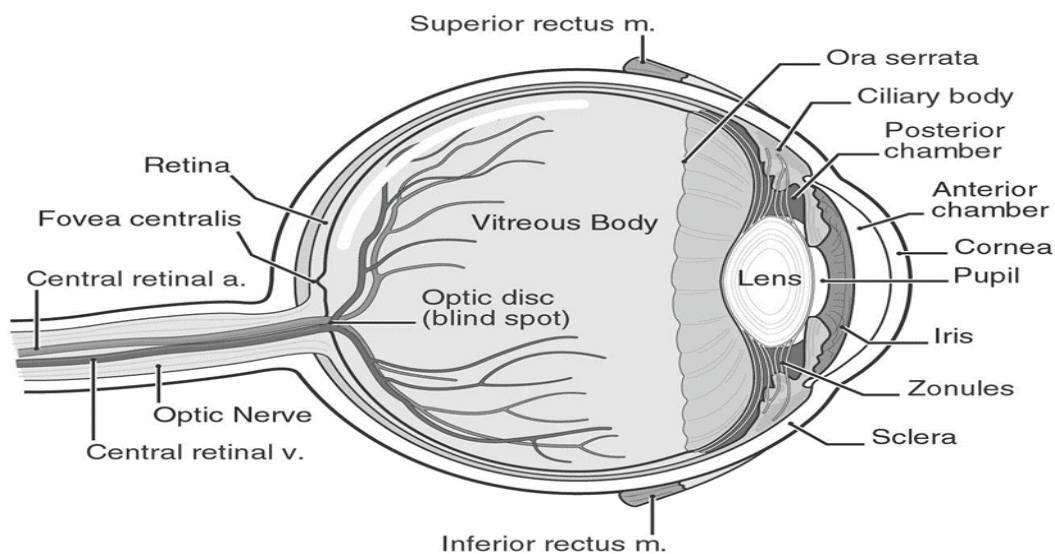


Figure 1:- Anatomy of human eye.

The posterior section contains the tissue layer, bodily fluid, choroid, sclera, and also the cranial nerve. The tissue layer may be a multi-layered sensory, photosensitive tissue that lines the rear of the attention. It consists of a neural layer, pigment animal tissue, and a lot of photos-receptors (rods and cones) that capture and after convert lightweight rays into electrical impulses. Such impulses are transferred by the cranial nerve to brain wherever pictures are shaped. The bodily fluid may be a jelly-like substance between the tissue layer and lens. This colloidal gel matrix consists of mucopolysaccharide, proteoglycans, and albuminoid fibrils. Separated from the anterior section by tissue layer, the vitreous is joined to the tissue layer via ligaments. Choroid coat may be an extremely vascularized tissue settled between the tissue layer and sclerotic coat. Its major perform is to supply nourishment to the photoreceptor cells within the tissue layer. Sclerotic coat is that the whitish outmost layer, close the world, and is named the "white of the attention." it's composed of albuminoid bundles, mucopolysaccharides, and elastic fibres. This tissue acts as a principal protect to shield the intraocular contents. The scleral tissue is regarding ten times a lot of porous than the tissue layer and a minimum of half as porous because the mucous membrane. Hence, permeants will diffuse and enter the posterior segment through the transscleral route.

ROUTE OF ADMINISTRATION OF DRUG

- Instillation into conjunctival sac
- Subconjunctival injection
- Sub tenon's injection
- Retrobulbar injection
- Peribulbar injection
- Intraocular injection
- Systemic administration

Ophthalmic diseases square measure primarily treated conventionally by medications administered via either the topical or general route. Topical application remains the foremost most well-liked route because of simple administration, low cost, and patient compliance. It's usually helpful within the treatment of anterior phase disorders.^[4] Drug delivery to the posterior phase still may be a major challenge to pharmaceutical scientists. Anatomical and physiological barriers hinder drug entry into posterior ocular tissues like membrane and choroid coat. Once topical instillation, an oversized fraction (about 90%) of the applied dose is lost because of nasolacrimal evacuation, tear dilution, and tear turnover, resulting in poor ocular bioavailability. But five-hitter of the administered dose reaches the bodily fluid once topical administration.^[5] Frequent dosing is needed, that ultimately ends up in patient discomfort and inconvenience. 2 major absorption routes are planned for medicine instilled via topical route: membrane route (cornea-aqueous humor-intraocular tissues) and noncorneal route (conjunctiva-sclera-choroid/retinalpigment epithelial tissue [RPE]). The

popular mode of absorption depends on the chemical science properties of the permeating.^[6,7]

Conventional topical formulations need frequent giant doses to provide therapeutic amounts within the back of the attention. Therefore, oral delivery alone^[8-10] or in combination with topical delivery^[11] has conjointly been investigated as a result of the oral route is taken into account as noninvasive and high in patient compliance, particularly for chronic retinal disorders. High doses square measure needed to realize important amounts within the membrane.

Such high doses, however, cause general adverse effects, and safety and toxicity become a significant concern. Oral administration isn't predominant and should be extremely useful given that the drug possesses high oral bioavailability. yet, molecules in circulation ought to be able to cross the blood-aqueous barrier (BAB) and BRB once oral administration.

Systemic administration is usually most well-liked for the treatment of posterior phase disorders. a significant disadvantage with this route, however, is that it solely permits I Chronicles to five of administered drug into the vitreous chamber. once general administration, the supply of drug is restricted by the BAB and BRB, that square measure the key barriers for anterior phase and posterior phase ocular drug delivery, severally. The BAB consists of 2 distinct cell layers: the epithelial tissue of the iris/ciliary blood vessels and also the nonpigmented ciliary epithelial tissue. each layers stop drug entry into the intraocular tissues, together with bodily fluid, thanks to the presence of tight junctions.^[12] in a very similar manner, BRB prevents drug entry from blood into the posterior phase. BRB consists of 2 types: retinal capillary epithelium cells (inner BRB) and RPE cells (outer BRB) . RPE may be a monolayer of extremely specialised cells sandwiched between neural membrane and also the choroid coat. It by selection transports molecules between photoreceptors and choriocapillaris.^[13] Tight junctions of RPE, however, conjointly prohibit animate thing drug transport.

Drug entry into the posterior ocular tissues is especially ruled by the BRB. it's by selection porous to extremely hydrophobic drug molecules. to take care of high drug concentrations, frequent dosing is important, which frequently ends up in general adverse effects.^[14] Drawbacks like lack of adequate ocular bioavailability and failure to deliver therapeutic drug concentration to the membrane diode ophthalmic scientists to explore various administration routes. Over the past decade, IVT injections have drawn important attention to scientists, researchers, and physicians. This technique involves injection of the drug resolution directly into the vitreous via the pars plana employing a 30-G needle. This route provides higher drug concentrations within the vitreous and membrane. not like different routes, the drug will be directly injected into the vitreous cavity; but, drug

distribution isn't uniform. though little molecules will apace diffuse throughout the vitreous fluid, the distribution of macromolecules is restricted or restricted. once IVT administration, drug elimination depends on the relative molecular mass of the compound furthermore because the pathophysiological condition.^[15] for instance, macromolecules, that square measure linear and globular-shaped compounds (especially supermolecule and amide drugs) with molecular weights between forty and seventy kDa, tend to cause longer retention within the body fluid.^[16] The half-life of the drug within the vitreous fluid is additionally a significant determinant of therapeutic efficaciousness. Elimination of a drug once IVT administration might occur via the anterior or posterior route. The anterior route of elimination involves drug diffusion to the binary compound from the body fluid via zonular areas followed by elimination through binary compound turnover and structure blood flow. On the opposite hand, the posterior route of elimination involves drug transport across the BRB, that necessitates optimum passive permeability or transport. Consequently, drug molecules with higher relative molecular mass and hydrophilicity tend to be preserved within the body fluid for extended periods because of longer half-lives of the compounds.^[13] though IVT administration is advantageous in achieving larger drug concentrations within the membrane, frequent administration is usually related to complications like endophthalmitis, visual defect, and IVT haemorrhages, resulting in the increasing in patient outcome.^[17] Periocular administration has conjointly been thought of as AN economical route for drugdelivery to the posterior phase. Periocular refers to the fringe of the attention or the region encompassing the attention. This route includes peribulbar, posterior juxta scleral, retro- neural structure, subtenon, and subconjunctival routes. medicine administered by the periocular route will reach the posterior phase of the attention by 3 completely different pathways: transscleral pathway, circulation through the choroid coat, and anterior pathway through the tear film, cornea, bodily fluid, and body fluid.^[18]

Subconjunctival injection involves the introduction of a full of life ingredient below the mucous membrane. mucous membrane epithelial tissue is a rate-limiting barrier for the porosity of soluble compounds. As a result, the transscleral pathway bypasses the cornea-conjunctiva barrier. numerous dynamic, static, and metabolic barriers, how- ever, impede drug entry to the rear of the attention. many publications reportable speedy drug elimination via these pathways once subconjunctival administration.^[19-21] Therefore, most of the administered dose drains into the circulation, resulting in poor ocular bioavailability. However, molecules that escape mucous membrane vasculature might go through albuginea and membrane and ultimately reach the neural membrane and photoreceptor cells. albuginea offers less resistance to drug transport and is additional permeable than the cornea.^[22] In contrast to tissue layer and mucous membrane tissues,

scleral perm ableness is freelance of lipophilicity/hydrophobicity however depends on the molecular radius.^[13, 23] On the opposite hand, high choroidal blood flow will cut back substantial fractions of the dose reaching the neural membrane. Moreover, BRB conjointly hinders drug convenience to the photoreceptor cells. though the periocular route is taken into account appropriate for sustained-release drug delivery systems, many anterior phase complications, like multiplied IOP, cataract, hyphema, strabismus, and tissue layer decompensation, are determined.^[24,25] Subtenon injection typically involves injection into the tenon's capsule settled around the higher portion of the attention and into the belly of the superior rectus muscle. The tenon's capsule may be a fibrous membrane that covers the world from the tissue layer margin to the nervus opticus. A blunt-tipped tubing needle is usually inserted into the tenon's capsule once a section into the sub tenon's area. this method is wide used throughout physiological condition for ocular surgery as a result of the tubing approach reduces sharp-needle complications.^[22] Retrobulbar injections typically involve the injection within the cone-shaped compartment among the muscle muscles and contractile organ septa. These injections offer higher native drug concentrations with negligible influence on IOP. The peribulbar route involves the injection within the animate thing areas of the muscle muscles and their contractile organ septa. though drug administration through the peribulbar route is safer, it's less effective than the retrobulbar route. Posterior juxta scleral injection employing a blunt-tipped bowed tubing delivers the drug directly onto the outer surface of albuginea. This route might enable sustained delivery to the macula. Retrobulbar injections square measure thought of the foremost economical among all periocular routes however square measure related to serious complications, like retrobulbar haemorrhage, globe perforation, and metastasis arrest.

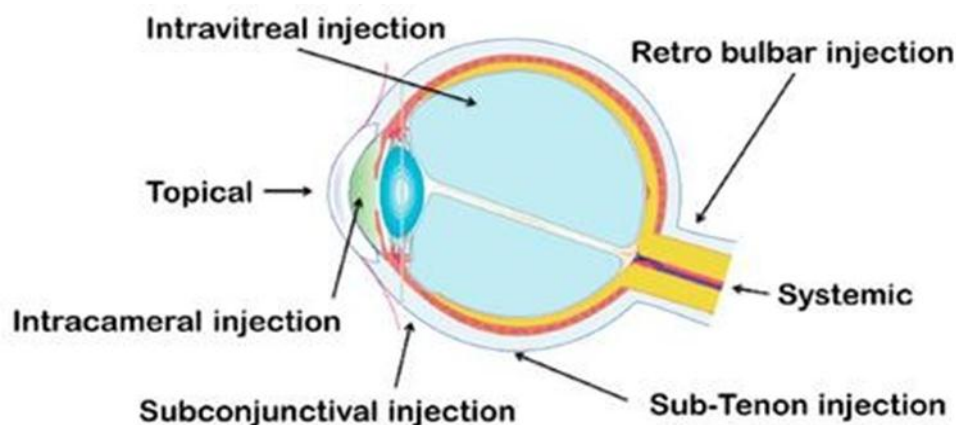


Figure 2:- Route of administration of drug.

Conventional Type:-The conventional drug delivery system is the absorption of the drug across a biological membrane, whereas the targeted release system releases the drug in a dosage form. Targeted drug delivery systems have been developed to optimize regenerative techniques. Topical drop instillation into the lower precorneal pocket could be a patient compliant and wide counselled route of drug administration. However, most of the locally administered dose is lost thanks to reflex blinking and solely 2 hundredth ($-7 \mu\text{L}$) of instilled dose is maintained within the precorneal pocket.^[26] Concentration of drug on the market within the precorneal space acts as a propulsion for its passive diffusion across membrane. However, for economical ocular drug delivery with eye drops, high membrane permeation with longer drug membrane contact time is needed. Many efforts are created toward up precorneal continuance and membrane penetration. To enhance membrane permeation iontophoresis, prodrugs, ion-pair forming agents and cyclodextrins square measure employed.^[27-31] There's a good vary of ophthalmic product on the market within the market out of that around seventieth of prescriptions embrace standard eye drops. The explanation is also thanks to simple bulk scale producing, high patient acceptableness, drug product efficaciousness, stability and price effectiveness.

Eye drops Solution- Topical drops area unit the foremost convenient, safe, directly active, patient compliant and non-invasive mode of ocular drug administration. A watch drop answer provides a pulse drug permeation post topical drop instillation, once that its concentration quickly declines. The mechanics of drug concentration decline could follow associate degree approximate initial order. Therefore, to boost drug contact time, permeation and ocular bioavailability; varied additives is also additional to topical eye drops like viscousness enhancers, permeation enhancers and cyclodextrins. Viscousness enhancers improve precorneal continuance and bioavailability upon topical drop administration by enhancing formulation viscousness. Samples of viscousness enhancers embrace group alkyl radical polyose, group ethyl group polyose, Na carboxy alkyl radical polyose, hydroxypropyl alkyl radical polyose and

polyalcohol.^[32-34] Permeation enhancers improve tissue layer uptake by modifying the tissue layer integrity. Different additives like chelating agents, preservatives, surface active agents and digestive juice salts were studied as potential permeation enhancers. Benzalkonium chloride, polyoxyethylene glycol ethers (lauryl, stearyl and oleyl), ethylenediamine tetra ethanoic acid sodium salt, Na taurocholate, saponins and cremophor EL are the samples of permeation enhancers investigated for rising ocular delivery.^[35-37] Addition of permeation enhancers to ocular solutions improves ocular drug bioavailability however few studies unconcealed a neighbourhood toxicity with permeation enhancers.^[38] Hence, analysis continues to be being conducted to change the result of permeation enhancers and measure their safety on tissue layer tissues. Hornof et al^[39] proved that polycarbophil-cysteine as AN excipient failed to harm the tissue layer tissue integrity and prompt that it may well be safe for ocular formulations. Cyclodextrins act as carriers for hydrophobic drug molecules in solution. This helps to deliver medication to the surface of biological membrane. extremely oleophilic biological membrane has abundant lower affinity towards hydrophilic cyclodextrins. Therefore, cyclodextrins stay in solution and therefore the hydrophobic drug is absorbed by the biological membrane. optimum bioavailability was achieved for eye drops with cyclodextrins concentration of $< 15\%$.^[40] Different applications of cyclodextrins in eye drop formulation were recently reviewed and represented very well elsewhere by Cholkar et al.^[41]

Among these approaches, viscousness enhancers and cyclodextrins suffer from the disadvantage of precorneal loss. within the case of penetration enhancers, care ought to be taken within the choice because of high sensitivity of ocular tissues. Hence, it results in development of different typical formulations approaches with inert carrier systems for ocular delivery of medical specialty. typical ocular formulations like emulsions, suspensions, and ointments area unit developed to boost solubility, precorneal duration and ocular bioavailability of medication. within the current era of technology, these typical formulations still retain their place, importance

and capture the market at massive. However, these formulations area unit related to varied aspect effects like ocular irritation, redness, inflammation, vision interference and stability issues.^[42] Currently, analysis is being conducted to boost in vivo performance of those carrier systems and to reduce their aspect effects.^[43]



Figure 3:- Demonstration of eye drop.

Emulsions:-An emulsion based mostly formulation approach offers a plus to enhance each solubility and bioavailability of medicine. There are 2 varieties of emulsions that are commercially exploited as vehicles for active pharmaceuticals: oil in water (o/w) and water in oil (w/o) emulsion systems.^[44] For ophthalmic drug delivery, o/w emulsion is common and wide most well-liked over w/o system. the explanations embrace less irritation and higher ocular tolerance of o/w emulsion. Restasis™, Refresh Endura® (a non-medicated emulsion for eye lubrication) and AzaSite® are the samples of presently marketed ocular emulsions within the U.S many studies have incontestable relevancy of emulsions in up precorneal continuance, drug membrane permeation, providing sustain drug unharness and thereby enhancing ocular bioavailability.^[45]

In a recent study, Tajika et al^[46] incontestable improved medication activity of anti-inflammatory drug spinoff, 0.05% [3H] difluprednate, with emulsion as vehicle. Results confirmed that within the rabbit eye, emulsion may deliver drug to the anterior ocular tissues with touch of drug reaching posterior tissues following single and multiple topical drop instillation. Single and multiple topical drop instillation studies disclosed highest radiation in tissue layer followed by iris-ciliary body > retina-choroid > mucosa > albuginea > humour > lens > and body fluid. Post single drop administration, T_{max} for tissue layer, mucosa, lens, iris-ciliary body, binary compound and body fluid was 0.5 h whereas for retina-choroid was one hr. Negligible quantity of drug was quantified in circulation. With continual dose instillation, T_{max} for lens and retina-choroid was eight and 0.5 h, severally. once 168 h, a complete dose of roughly ninety 9.5% of radiation was excreted in body waste and BM. This study suggests difluprednate emulsion as a possible candidate for treating anterior ocular inflammations. Emulsions with supermolecule additives like soyabean emulsifier, stearyl amine were evaluated as carrier systems for azithromycin to demonstrate higher

many makes an attempt are being created to deliver medication to posterior ocular tissues with typical formulations. within the following sections, makes an attempt are created to explain the recent efforts created to boost in vivo performance of typical ocular formulation and cut back their aspect effects.

ocular performance and bioavailability.^[47] A comparative study for azithromycin resolution vs emulsion at totally different doses (3, five and ten mg/mL azithromycin) was studied for tear elimination characteristics. in vivo studies were conducted in rabbits with topical drop administration. Emulsion, not solely ascertained to behave as a vehicle for azithromycin however additionally slowed drug unharness, improved its chemical stability and precorneal continuance. in addition, emulsion formulation improved the chemical stability ($t_{1/2}$) of azithromycin at pH scale five.0 and 7.0 relative to binary compound solutions. Altogether, results counsel that supermolecule emulsion might be a promising vehicle for ocular drug delivery.

Suspension:- Suspensions are another category of non-invasive ocular topical drop drug carrier systems. Suspension is also outlined as dispersion of finely divided insoluble API in associate degree a solvent consisting of an appropriate suspending and dispersing agent. In alternative words, the carrier solvent system is a saturated solution of API. Suspension particles retain in precorneal pocket and thereby improve drug contact time and length of action relative to drug solution. length of drug action for suspension is particle size dependent. Smaller size particle replenishes the drug absorbed into ocular tissues from precorneal pocket. whereas on the opposite hand, larger particle size helps retain particles for extended time and slow drug dissolution.^[48] Thus, an optimum particle size is predicted to end in optimum drug activity. many suspension formulations are marketed worldwide to treat ocular microorganism infections. TobraDex® suspension is one among the wide counselled business product for subjects responding to steroid medical aid. TobraDex® could be a combination product of antibiotic, tobramycin (0.3%), and steroid, dexamethasone (0.1%). the most important downside of this business product is high viscousness. Recently, Scoper et al^[49] created makes an attempt to cut back the viscousness of TobraDex® and to boost its in

vivo pharmacokinetics alongside disinfectant activity. The principle behind developing this formulation was to boost the suspension formulation characteristics like quality, tear film dynamics and tissue permeation. The new suspension (TobraDex ST®) consists of tobramycin (0.3%), and steroid, dexamethasone (0.05%). Suspension subsidence studies showed that new formulation had terribly low subsidence over twenty-four h (3%) relative to marketed Tobra-Dex® (66%). Ocular distribution studies showed higher tissues concentrations of anti-inflammatory drug and antibiotic in rabbits treated with TobraDex ST® relative to TobraDex®. New suspension formulation was found to be simpler than TobraDex® against coccus aureus and Pseudomonas aeruginosa. Clinical studies in human subjects showed high dexamethasone concentrations in humour than TobraDex®. These results counsel that new suspension formulation to be another to marketed suspension. this is often as a result of the new suspension possesses higher formulation characteristics, Materia medica, disinfectant characteristic and patient compliance than marketed TobraDex® suspension. In another study, to treat dry eye, 4 wk, randomized, double cloaked, multicentre clinical trial clinical trials were conducted with rebamipide (OPC-12759) suspension.^[50] Suspension formulation at 2 totally different doses, i.e., 1 Chronicles and a pair of rebamipide were used for this study, wherever placebo served as management. The efficaciousness and safety of suspension formulation were determined in human subjects following topical instillation. All the topics receiving treatment with suspension rebamipide formulation according improvement of 64.1% and 54.9% severally than subjects receiving placebo. Dysgeusia, ocular irritation and nasopharyngitis adverse events were often discovered in 27.2%, 29.1% and 30.4% patients receiving placebo, 1 Chronicles and a pair of suspension, severally. Drug elicited adverse effects like eye irritation was discovered in 3.9%, 2.9% and 2.0% subjects receiving placebo, 1 Chronicles rebamipide and a pair of rebamipide severally. of these adverse effects were found to recover with none extra treatment. This four-week studies unconcealed that suspension formulations were well tolerated and each formulations were effective in treating dry eye. In some measures, of the 2 formulations, two rebamipide suspension was found to be simpler relative to a quarter suspension.

Ointments:- Ophthalmic ointments square measure another category of carrier systems developed for topical application. Ocular ointment contains of mixture of solid and a solid organic compound (paraffin) that encompasses a temperature at physiological ocular temperature (34 °C). the selection of organic compound relies on biocompatibility. Ointments facilitate to enhance ocular bioavailability and sustain the drug release^[51]. Vancomycin HCl (VCM) may be a glycopeptides antibiotic with a wonderful activity against aerobic and anaerobic gram-positive microorganism and methicillin and cephem resistant coccus aureus (MRSA).

In spite of higher activity of VCM, no applicable topical formulation was obtainable within the market. higher ocular tissue porosity of VCM wasn't expected in an exceedingly traditional eye however few clinical effects of VCM resolution were rumoured in ocular unwellness treatment. the explanation for the discovered effects was hypothesized thanks to broken ocular barrier system, which could have improved drug permeation. Fukuda et al^[52] studied the intraocular dynamics of antibiotic coordination compound ophthalmic ointments in rabbits. Thus, authors created tries to demonstrate ocular dynamics of VCM ophthalmic ointment (TN-011) with indications restricted to extraocular MRSA infections. The minimum growth restrictive concentration to treat MRSA bacterial infections was found to be 1.56 µg/g. in vivo studies were conducted in rabbits [normal vs bacillus subtilis (BS) group]. The bacillus subtilis cluster was developed in membrane by injecting baccalaureate resolution into the central portion of parenchyma. Treatment was by topical ocular ointment (1% VCM) administration to traditional and bacillus subtilis cluster rabbit eye. In traditional cluster, once fifteen min, VCM concentration in membrane of 12.04 ± 4.73 µg/g was earned at thirty min that was weakened to 0.49 ± 0.97 µg/g at one hundred twenty min. On the opposite hand, VCM concentrations in bacillus subtilis cluster membrane was 25.60 ± 11.01 µg/g once fifteen min and 3.68 ± 1.38 µg/g once 240 min of administration. The concentrations of VCM were maintained on top of MIC levels, in MRSA infection induced *Bacillus subtilis* cluster, a substantial profit to the patients from TN-011 is anticipated. In another study by Eguchi et al^[53], four totally different ointment formulation of antibiotic with variable concentrations (0.03%, 0.10%, 0.30% and 1.00%) were ready in 1:4 mixtures of liquid paraffin and Vaseline. The effectiveness of formulations was evaluated in rabbit model of MRSA redness infection once topical application. it absolutely was discovered that at low drug concentrations, i.e., 0.03% and 0.10%, varied infiltrates were found in corneas with abscesses. On the opposite hand, animals treated with zero.3% formulation showed no return of redness in any eye over fourteen d study amount. Therefore, 0.3% vancomycin ointment was instructed to be adequate and effective to resolve tissue layer MRSA redness.

Though wide effort is being place into analysis to enhance effectiveness, still there's a desire to beat bound drawbacks related to standard formulations. The on top of mentioned formulations: emulsion, suspension, and ointment square measure identified to cause ocular adverse effects like irritation, redness of eye and interference with vision. Also, chronic administration might increase general API handiness which can result in severe general complications.^[54-56] Formulations with preservatives additionally induce adverse reactions upon general absorption.^[57,58] Therefore, to beat formulation based mostly adverse effects and to deliver therapeutic amounts of drug in ocular tissues, analysis is currently being targeted on exploring and developing different

novel methods of ocular drug delivery. within the following sections, we've mentioned concerning the recent developments created in nanotechnology and controlled unleash devices in past decade to enhance ocular drug delivery.

Nano technology-based drug delivery Various drug delivery approaches are developed for treating ocular diseases of that nanotechnology based mostly approaches are concerned in anterior still as posterior portion treatment of eye. Particle size are appropriately developed in nanotechnology primarily based delivery system so as to confirm that it possesses adequate bioavailability, compatibility with ocular tissue, and lesser irritation.^[59] Occurrences of this nanotechnology based mostly ocular system the site safe, precise and supply doable targeting to the location. For the treatment of ocular surface various nanocarriers like nano micelles, nanoparticles, nanosuspensions, liposomes and dendrimers are developed, of which some show a promising improvement within the bioavailability.^[60]

Nanomicelles:- Nano micelles square measure nano-sized carriers wherever the therapeutic agents square measure developed into liquid clear solutions. it's composed of amphiphilic molecules and maybe these molecules square measure chemical compound or wetting agent primarily based.^[61] an excellent interest is shown in developing Nano micellar formulation for ocular this might ensue to the explanation that the dimensions is little, straightforward to formulate, drug encapsulation is high, and conjointly the solution is generated by hydrophilic nano micellar corona. Moreover, the micelles formulation improves the bioavailability of therapeutic moiety in ocular tissues and so their therapeutic outcomes square measure resulted to be higher. Demonstration of mixed nano micelles formulation resulted in well tolerated and fewer irritation. Nano micellar primarily based drug delivery could be a topical drop and comes under non-invasive route that is of gaining interest because of their smaller size, hydrophilic corona, retentive for extended time within the systemic circulation, and accumulation within the morbid tissues through EPR impact. surfactant and polymer choice ought to be applicable so as to help this Nano micellar technique to delivery medication at each anterior and further as posterior portion of eye.^{[59][62]}

Nanoparticles:- Nanoparticles delivery systems have potential applications for ocular drug delivery. Particulate carriers meet the fundamental needs of advanced ocular drug carriers, being nontoxic, non-immunogenic, biocompatible, uniform, and biodegradable during a foreseeable pace. additionally, they have the flexibility to supply protection for the delivered molecules whereas interacting with the ocular surface. intensive analysis efforts for current within the development of ophthalmic particulate delivery systems. The adhesive properties of those chemical compound systems contributed to the improvement of corneal

penetration of the drug as a result of the inflated increased of the drug within the pre- corneal environment.^[63]

Furthermore, surface modifications of nanoparticles with a sterically stabilising layer will modulate their *in-vivo* biodistribution and lower their tendency to combination with bio molecules. Longer residence times on the ocular surface are often achieved if the nanoparticles square measure coated with a muco-adhesive or charged polymer. In general, there's a drive for target-specific surface modifications supported the notion that each non coated and pegylated particulate systems square measure nonspecific in their interaction with cells and macromolecules.

PLA nanosphere colloidal suspensions containing acyclovir provided a marked sustained drug unharness within the humour and considerably higher levels of acyclovir compared to the free drug formulation. once loaded in PLA nano-spheres, acyclovir humour space underneath the curve was seven times higher compared to the free drug formulation space underneath the curve, whereas the pegylation of the nano-spheres nearly doubled this augmentation.^[64] The potential of chitosan nanoparticles for ocular drug delivery by work their interaction with the ocular mucosa *in-vivo* and additionally their toxicity in conjunctival cell cultures. Chitosan nanoparticles were stable upon incubation with enzyme and failed to have an effect on the mucin of glycoprotein dispersion. In-vivo studies showed that the amounts of Chitosan nanoparticles in tissue layer and mucous membrane were considerably higher for Chitosan nanoparticles than for an impression Chitosan nanoparticles answer, these amounts being fairly constant for up to 24 hrs.

Confocal studies recommend that nanoparticles penetrate into the tissue layer and conjunctival epithelia. Cell survival at 24 h when incubation with chitosan nanoparticles was high and therefore the viability of the recovered cells was close to 100 pc. Chitosan nanoparticles square measure promising vehicles for ocular drug delivery.^[65]

Nanosuspension:- Nanosuspensions are submicron colloidal dispersions of nanosized drug particles stabilized by surfactants.^[66] Nanosuspensions seem to be a promising approach for hydrophobic drug delivery and additionally act as a more robust formulation/dosage form when put next to standard solutions and suspensions. blessings of using this nanosuspension involve simple formulation, non-irritant, increased ocular bioavailability of insoluble drug in tears fluid, precorneal duration is prolonged, higher sterilization.^[67] it's believed that it's associate economical delivery system for hydrophobic drugs wherever the speed and extend of drug absorption isn't solely redoubled however additionally the drug action intensity with extended period is obtained. The key modification from

conventional formulations of suspensions is that the particle size distribution of the solid particles in nano-suspensions is usually less than 1 μm (*i.e.*, 0.1nm-1000nm), with an average particle size range between 200–600 nm. On the other hand, the particle diameter essential in best pharmaceutical suspensions is 1 to 50 μm. In nano-suspensions, the overall bioavailability is improved by an increase in surface area and saturation solubility via particle size reduction.^[68] when instillation the fine particles adhere to ocular tissues and there'll be a formation of depot to release the drug when a amount of your time. moreover, the larger area of the nanoparticles offers sufficient rate of drug release and maintains a good concentration of drug to accomplish a desired bioavailability.

Liposomes:- Liposomes are vesicles of lipid that have one or additional phospholipid bilayers and enclose an aqueous core. they typically have size-range of 0.08–10.00 μm. primarily based upon its size and also the variety of bilayers of phospholipid, liposomes could also be classified into tiny unilamellar vesicles of size vary between 10 and 100 nm, large unilamellar vesicles of the scale vary between 100 and 300 nm, and multilamellar vesicles, that contain over one bilayer of phospholipid.^[69,70] Liposomes have shown to be a perfect

ophthalmic drug delivery system as a result of it will encapsulate hydrophilic similarly as hydrophobic medicine and conjointly shows a really smart compatibility with the ocular tissues. many analysis studies have conjointly incontestable that liposomal ocular delivery is effective for each anterior and posterior segments.^[69] Li et al. developed a diclofenac sodium-loaded liposomal formulations with low mass chitosan (LCH) coating. Results demonstrated a small increase within the particle size with prolonged unharness of drug. Stability check results were acceptable. LCH-coated cyst showed AN increased retention and penetration through the membrane. No cases of ocular irritancy or toxicity were determined.^[71] Kaiser et al. developed nano-sized negatively charged cholesterol-fusing ocular liposomal formulations containing minocycline. Quasi-elastic light scattering showed unilamellar vesicles of terribly slim size vary. The formulations were slightly charged. Encapsulation potency studies demonstrated that about 2%–3% of the initial quantity of the drug was loaded. The formulations were non-toxic as analysed from the DNA fragmentation of the retina and conjointly might deliver 400th of the drug to retina following injection to the sub-conjunctiva.^[72]

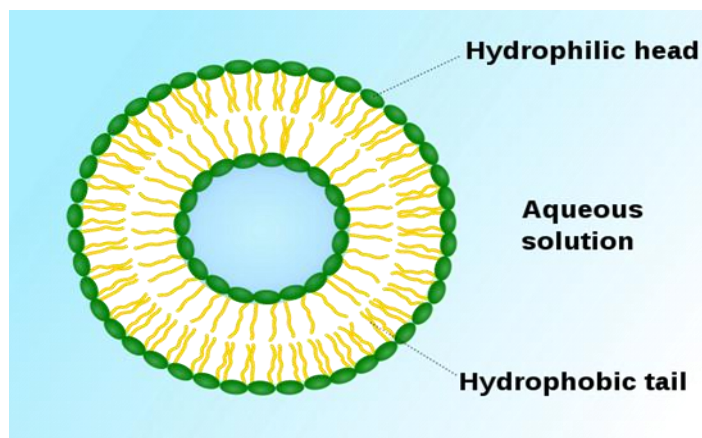


Figure 4:-Liposomes.

Dendrimers:- The macromolecular compounds within which an inner core is surrounded by a series of branches square measure named as dendrimers. Dendrimers have sizes in millimicron vary and may terribly simply be ready and functionalized. Also, dendrimers demonstrate the power to point out varied copies of surface teams for the method of recognition biologically. Hence, they're an awfully engaging technique for drug delivery.^[73,74-76] Dendrimers, being nano-sized polymeric systems square measure extremely branched and angular, with variable molecular weights and terminal useful teams like amine, hydroxyl, or carboxyl teams that will be utilized in conjugating targeting moieties.^[69,77] PAMAM (poly(amidoamide)) dendrimers square measure greatly used in ocular delivery of drugs.^[78] within the delivery of drugs, dendrimers square measure used as carrier systems for drugs, and for this, the relative molecular

mass, size, surface charge, molecular geometry, and useful cluster ought to be properly selected. exaggerated branching of dendrimers permits incorporation of a bigger form of drugs, each hydrophobic and hydrophilic. Such branched dendrimer systems are reported to point out promising ends up in ocular delivery.^[79,69,78,80]

Implants:- Intraocular implants are used specifically to produce controlled release of the drug over an extended period. an ocular implant helps to bypass intraocular injections and additionally complication related to it.^[69] For posterior tissue drug delivery, implants by surgical process through creating an incision placed intravitreally at the pars plana set at anterior to tissue layer and posterior to lens. so being a invasive route of delivery, implantation is gaining interest as a result of blessings related to this device which has emotional drug at

therapeutic level to pathologic tissues, sustained release, circumvent barriers and side effects is reduced.^[81] numerous implantable devices are designed for treating diseases particularly chronic vitreoretinal as ocular delivery system.

Microneedles:- Microneedle based technique is an emerging and minimally invasive mode of drug delivery to posterior ocular tissues. This technique may provide efficient treatment strategy for vision threatening posterior ocular diseases such as age-related macular degeneration, diabetic retinopathy and posterior uveitis. This new microneedle-based administration strategy may reduce the risk and complications associated with intravitreal injections such as retinal detachment, haemorrhage, cataract, endophthalmitis and pseudo endophthalmitis.

This technique is efficient in treating the vision menacing posterior diseases such as diabetic retinopathy, macular degeneration and posterior uveitis. Microneedle strategy can circumvent the BRB (blood retinal barrier) and helps in delivering the therapeutic agents to the retina.^[69] Microneedles to biological membranes creates micro-dimension transport pathway and also enhances the permeability of drugs across the barriers. Plenty of approaches have been developed for fabricating the microneedles in variety of size, shapes, materials and/or configurations. It has been developed as a physical method to avoid most of the side effects produced by the conventional injections in ocular delivery system. Being a custom designed device, these microneedles can penetrate into sclera only few hundred microns level, thus avoids the damage to deeper tissues of ocular. These microneedles deposit carrier system and/or therapeutic agents into sclera and a narrow space called “suprachoroidal space” (SCS) between the sclera and choroid. Therefore, puncturing the sclera and drug depositing into it or facilitating the SCS may cause diffusion into deeper ocular tissues. Several microneedles are designed and various drug delivery routes are also evaluated.^[69,81] A recent occurrence of microneedles for delivering the therapeutic agents to SCS (suprachoroidal space) is studied to be better targeting approach. It is developed with length same as that of sclera thickness, for a perpendicular insertion to sclera-choroid junction and referred as invasive method.^[82,83]

Contact Lens:- Contact lenses are thin, curve-shaped plastic discs designed to be placed over the cornea.^[84] placing inserting over the membrane, contact lenses adhere to the surface of the cornea as a result of interfacial surface tension. each the cornea and make contact with lens area unit separated from one another by a thin tear fluid layer known as post lens tear film. In general, contact lenses are ready with polymers like silicone gel (N,N,N,N-dimethylacrylamide, 3-methacryloxypropyltris(trimethylsiloxy) silane, bisalpha,omega-[methacryloxypropyl] poly dimethyl

siloxane, 1-vinyl-2-pyrrolidone, and ethylene glycol dimethacrylate) and poly (hydroxyethyl methacrylate) (p-HEMA).^[85,86]

It produces better ocular bioavailability than the topical drops. And also, by suspending these nanoparticles in thermogelling polymers the residence time can be prolonged. This approach serves a major benefit of prolonging the residence time which exists few minutes with eye drops in post tear films. Thus becomes an attractive alternative to the topical instilled eye drops.^[87] Since the residence time is lengthened by this approach the permeation of the drug is also higher at the targeted tissue through cornea. Contact lenses also offer advantages such as by increasing the transport of drug into cornea as well as conjunctiva. Meanwhile the drawbacks of contact lenses are that it causes toxicity to ocular.^{[88][89]}

CONCLUSION

The advanced nature in physiology of eye and also the barriers poignant the effectivity of existing approaches had cause the event of novel therapies. Administration of drug solutions as topical drop with conventional formulations was related to some drawbacks that initiated the introduction of various carrier systems for ocular delivery. many nanotechnologies based mostly carrier systems are being developed and studied at large like nanoparticles, liposomes, nano micelles, nanosuspensions and dendrimers. Few of those area unit commercially factory-made at massive scale and are applied clinically. nanotechnology is benefiting the patient body by minimizing the drug induced toxicities and vision loss. Recent technological advancement has modified the sector of ocular drug delivery from conventional drops to sustained release and targeted ocular delivery systems. within the recent era of technology, combinatorial approach looks to be attention of analysis within the development of safe and economical ophthalmic drug delivery systems.

REFERENCES

- Figure 1- [https:// images. app. goo. gl /uQZ7qMsWpCfYqWg6A](https://images.app.goo.gl/uQZ7qMsWpCfYqWg6A)
 Figure 2- <https://images.app.goo.gl/nz1DsbiuE1kuw7rE7>
 Figure 3- [https:// images. app. goo.gl/ YZMCtnqMoPPUNeCm7](https://images.app.goo.gl/YZMCtnqMoPPUNeCm7)
 Figure4- [https:// images. app. goo. gl/ 9o3g7uBaXF2TCH3Y8](https://images.app.goo.gl/9o3g7uBaXF2TCH3Y8)
1. Vadlapudi AD, Patel A, Cholkar K, Mitra A. Recent patents on emerging therapeutics for the treatment of glaucoma, age related macular degeneration and uveitis. *Rec Pat Biomed Eng*, 2012; 5(1): 83–101.
 2. Barar J, Asadi M, Mortazavi-Tabatabaei SA, Omidi Y. Ocular drug delivery; impact of in vitro cell culture models. *J Ophthalm Vis Res*, 2009; 4(4): 238–252.

3. Dua HS, Faraj LA, Said DG, Gray T, Lowe J. Human corneal anatomy redefined: a novel pre-Descemet's layer (Dua's layer). *Ophthalmology*, 2013; 120(9): 1778–1785.
4. Lee VH, Robinson JR. Topical ocular drug delivery: recent developments and future challenges. *J OculPharmacol*, 1986; 2(1): 67–108.
5. Hughes PM, Olejnik O, Chang-Lin JE, Wilson CG. Topical and systemic drug delivery to the posterior segments. *Adv Drug Deliv Rev*, 2005; 57(14): 2010–2032.
6. Gaudana R, Jwala J, Boddu SH, Mitra AK. Recent perspectives in ocular drug delivery. *Pharm Res*, 2009; 26(5): 1197–1216.
7. Ahmed I, Patton TF. Importance of the noncorneal absorption route in topical ophthalmic drug delivery. *Invest Ophthalmol Vis Sci*, 1985; 26(4): 584–587.
8. Santulli RJ, Kinney WA, Ghosh S, et al. Studies with an orally bioavailable alpha V integrin antagonist in animal models of ocular vasculopathy: retinal neovascularization in mice and retinal vascular permeability in diabetic rats. *J Pharmacol Exp Ther*, 2008; 324(3): 894–901.
9. Shirasaki Y, Miyashita H, Yamaguchi M. Exploration of orally available calpain inhibitors. Part 3. Dipeptidyl alpha-ketoamide derivatives containing pyridine moiety. *Bioorg Med Chem*, 2006; 14(16): 5691–5698.
10. Kampougeris G, Antoniadou A, Kavouklis E, Chrysouli Z, Giamarellou H. Penetration of moxifloxacin into the human aqueous humour after oral administration. *Br J Ophthalmol*, 2005; 89(5): 628–631.
11. Sakamoto H, Sakamoto M, Hata Y, Kubota T, Ishibashi T. Aqueous and vitreous penetration of levofloxacin after topical and/or oral administration. *Eur J Ophthalmol*, 2007; 17(3): 372–376.
12. Pitkanen L, Ranta VP, Moilanen H, Urtti A. Permeability of retinal pigment epithelium: effects of permeant molecular weight and lipophilicity. *Invest Ophthalmol Vis Sci*, 2005; 46(2): 641–646.
13. Urtti A. Challenges and obstacles of ocular pharmacokinetics and drug delivery. *Adv Drug Deliv Rev*, 2006; 58(11): 1131–1135.
14. Duvvuri S, Majumdar S, Mitra AK. Drug delivery to the retina: challenges and opportunities. *Expert Opin Biol Ther*, 2003; 3(1): 45–56.
15. Mitra AK, Duvvuri S. Drug delivery to the eye. In: J Fischbarg, ed. *The Biology of the Eye*. New York: Academic Press, 2006: 307–351.
16. Marmor MF, Negi A, Maurice DM. Kinetics of macromolecules injected into the subretinal space. *Exp Eye Res*, 1985; 40(5): 687–696.
17. Ausayakhun S, Yuvaves P, Ngamtiphakom S, Prasitsilp J. Treatment of cytomegalovirus retinitis in AIDS patients with intravitreal ganciclovir. *J Med Assoc Thai*, 2005; 88(Suppl 9): 15–20.
18. Ghate D, Edelhofer HF. Ocular drug delivery. *Expert Opin Drug Deliv*, 2006; 3(2): 275–287.
19. Hosseini K, Matsushima D, Johnson J, et al. Pharmacokinetic study of dexamethasone disodium phosphate using intravitreal, subconjunctival, and intravenous delivery routes in rabbits. *J OculPharmacolTher*, 2008; 24(3): 301–308.
20. Kim SH, Csaky KG, Wang NS, Lutz RJ. Drug elimination kinetics following subconjunctival injection using dynamic contrast-enhanced magnetic resonance imaging. *Pharm Res*, 2008; 25(3): 512–520.
21. Weijtens O, Feron EJ, Schoemaker RC, et al. High concentration of dexamethasone in aqueous and vitreous after subconjunctival injection. *Am J Ophthalmol*, 1999; 128(2): 192–197.
22. Raghava S, Hammond M, Kompella UB. Periocular routes for retinal drug delivery. *Expert Opin Drug Deliv*, 2004; 1(1): 99–114.
23. Prausnitz MR, Noonan JS. Permeability of cornea, sclera, and conjunctiva: a literature analysis for drug delivery to the eye. *J Pharm Sci*, 1998; 87(12): 1479–1488.
24. Chew EY, Glassman AR, Beck RW, et al. Ocular side effects associated with peribulbar injections of triamcinolone acetonide for diabetic macular edema. *Retina*, 2011; 31(2): 284–289.
25. Castellarin A, Pieramici DJ. Anterior segment complications following periocular and intraocular injections. *Ophthalmol Clin North Am*, 2004; 17(4): 583–590.
26. Schoenwald RD. Ocular drug delivery. Pharmacokinetic considerations. *Clin Pharmacokinet*, 1990; 18: 255–269.
27. Vaka SR, Sammeta SM, Day LB, Murthy SN. Transcorneal iontophoresis for delivery of ciprofloxacin hydrochloride. *Curr Eye Res*, 2008; 33: 661–667.
28. Tirucherai GS, Dias C, Mitra AK. Corneal permeation of ganciclovir: mechanism of ganciclovir permeation enhancement by acyl ester prodrug design. *J OculPharmacolTher*, 2002; 18: 535–548.
29. Gunda S, Hariharan S, Mitra AK. Corneal absorption and anterior chamber pharmacokinetics of dipeptide monoester prodrugs of ganciclovir (GCV): in vivo comparative evaluation of these prodrugs with Val-GCV and GCV in rabbits. *J OculPharmacolTher*, 2006; 22: 465–476.
30. Gallarate M, Chirio D, Bussano R, Peira E, Battaglia L, Baratta F, Trotta M. Development of O/W nanoemulsions for ophthalmic administration of timolol. *Int J Pharm*, 2013; 440: 126–134.
31. Tirucherai GS, Mitra AK. Effect of hydroxypropyl beta cyclodextrin complexation on aqueous solubility, stability, and corneal permeation of acyl ester prodrugs of ganciclovir. *AAPS PharmSciTech*, 2003; 4: 45.
32. Vulovic N, Primorac M, Stupar M, Brown MW, Ford JL. Some studies on the preservation of indometacin suspensions intended for ophthalmic use. *Pharmazie*, 1990; 45: 678–679.

33. Meseguer G, Buri P, Plazonnet B, Rozier A, Gurny R. Gamma scintigraphic comparison of eyedrops containing pilocarpine in healthy volunteers. *J OculPharmacolTher*, 1996; 12: 481–488.
34. Gebhardt BM, Varnell ED, Kaufman HE. Cyclosporine in collagen particles: corneal penetration and suppression of allograft rejection. *J OculPharmacolTher*, 1995; 11: 509–517.
35. Saettone MF, Chetoni P, Cerbai R, Mazzanti G, Braghiroli L. Evaluation of ocular permeation enhancers: in vitro effects on corneal transport of four beta-blockers, and in vitro/in vivo toxic activity. *Int J Pharm*, 1996; 142: 103–113.
36. van der Bijl P, van Eyk AD, Meyer D. Effects of three penetration enhancers on transcorneal permeation of cyclosporine. *Cornea*, 2001; 20: 505–508.
37. Burgalassi S, Chetoni P, Monti D, Saettone MF. Cytotoxicity of potential ocular permeation enhancers evaluated on rabbit and human corneal epithelial cell lines. *Toxicol Lett*, 2001; 122: 1–8.
38. Keister JC, Cooper ER, Missel PJ, Lang JC, Hager DF. Limits on optimizing ocular drug delivery. *J Pharm Sci*, 1991; 80: 50–53.
39. Hornof MD, Bernkop-Schnürch A. In vitro evaluation of the permeation enhancing effect of polycarbophil-cysteine conjugates on the cornea of rabbits. *J Pharm Sci*, 2002; 91: 2588–2592.
40. Kurz D, Ciulla TA. Novel approaches for retinal drug delivery. *Ophthalmol Clin North Am*. 2002;15:405–410.
41. Cholkar K, Patel SP, Vadlapudi AD, Mitra AK. Novel strategies for anterior segment ocular drug delivery. *J OculPharmacolTher*, 2013; 29: 106–123.
42. Mannermaa E, Vellonen KS, Urtti A. Drug transport in corneal epithelium and blood-retina barrier: emerging role of transporters in ocular pharmacokinetics. *Adv Drug Deliv Rev*, 2006; 58: 1136–1163.
43. Shen J, Gan L, Zhu C, Zhang X, Dong Y, Jiang M, Zhu J, Gan Y. Novel NSAIDs ophthalmic formulation: flurbiprofen axetil emulsion with low irritancy and improved anti-inflammation effect. *Int J Pharm*, 2011; 412: 115–122.
44. Vandamme TF. Microemulsions as ocular drug delivery systems: recent developments and future challenges. *Prog Retin Eye Res*, 2002; 21: 15–34.
45. Liang H, Brignole-Baudouin F, Rabinovich-Guilatt L, Mao Z, Riancho L, Faure MO, Warnet JM, Lambert G, Baudouin C. Reduction of quaternary ammonium-induced ocular surface toxicity by emulsions: an in vivo study in rabbits. *Mol Vis*, 2008; 14: 204–216.
46. Tajika T, Isowaki A, Sakaki H. Ocular distribution of difluprednate ophthalmic emulsion 0.05% in rabbits. *J OculPharmacolTher*, 2011; 27: 43–49.
47. Liu Y, Lin X, Tang X. Lipid emulsions as a potential delivery system for ocular use of azithromycin. *Drug Dev Ind Pharm*, 2009; 35: 887–896.
48. Lang J, Roehrs R, Jani R. Remington: The Science and Practice of Pharmacy. 21. Philadelphia: Lippincott Williams & Wilkins Ophthalmic preparations, 2009; p. 856.
49. Scoper SV, Kabat AG, Owen GR, Stroman DW, Kabra BP, Faulkner R, Kulshreshtha AK, Rusk C, Bell B, Jamison T, Bernal-Perez LF, Brooks AC, Nguyen VA. Ocular distribution, bactericidal activity and settling characteristics of TobraDex ST ophthalmic suspension compared with TobraDex ophthalmic suspension. *Adv Ther*, 2008; 25: 77–88.
50. Kinoshita S, Awamura S, Oshiden K, Nakamichi N, Suzuki H, Yokoi N. Rebamipide (OPC-12759) in the treatment of dry eye: a randomized, double-masked, multicenter, placebo-controlled phase II study. *Ophthalmology*, 2012; 119: 2471–2478.
51. Sasaki H, Yamamura K, Mukai T, Nishida K, Nakamura J, Nakashima M, Ichikawa M. Enhancement of ocular drug penetration. *Crit Rev Ther Drug Carrier Syst*, 1999; 16: 85–146.
52. Fukuda M, Hanazome I, Sasaki K. The intraocular dynamics of vancomycin hydrochloride ophthalmic ointment (TN-011) in rabbits. *J Infect Chemother*, 2003; 9: 93–96.
53. Eguchi H, Shiota H, Oguro S, Kasama T. The inhibitory effect of vancomycin ointment on the manifestation of MRSA keratitis in rabbits. *J Infect Chemother*, 2009; 15: 279–283.
54. Gray C. Systemic toxicity with topical ophthalmic medications in children. *Paediatric and Perinatal Drug Therapy*, 2006; 7: 23–29.
55. Ishibashi T, Yokoi N, Kinoshita S. Comparison of the short-term effects on the human corneal surface of topical timolol maleate with and without benzalkonium chloride. *J Glaucoma*, 2003; 12: 486–490.
56. Whitson JT, Ochsner KI, Moster MR, Sullivan EK, Andrew RM, Silver LH, Wells DT, James JE, Bosworth CF, Dickerson JE, Landry TA, Bergamini MV. The safety and intraocular pressure-lowering efficacy of brimonidine tartrate 0.15% preserved with polyquaternium-1. *Ophthalmology*, 2006; 113: 1333–1339.
57. Ayaki M, Yaguchi S, Iwasawa A, Koide R. Cytotoxicity of ophthalmic solutions with and without preservatives to human corneal endothelial cells, epithelial cells and conjunctival epithelial cells. *Clin Experiment Ophthalmol*, 2008; 36: 553–559.
58. Ayaki M, Iwasawa A, Yaguchi S, Koide R. Preserved and unpreserved 12 anti-allergic ophthalmic solutions and ocular surface toxicity: in vitro assessment in four cultured corneal and conjunctival epithelial cell lines. *Biocontrol Sci*, 2010; 15: 143–148.
59. Ashaben Patel, Kishore Cholkar, VibhutiAgrahari, Ashim K Mitra. Ocular drug delivery systems: An overview. *World Journal of Pharmacology*, 2013; 2(2): 47-64.

60. Anchal Tyagi, Pramod Kumar Sharma, Rishabha Malviya. Novel technology and future prospects of ocular drug delivery. *Journal of basic pharmacology and toxicology*, 2017; 1(4): 1-8.
61. Gupta AK, Madan S, Majumdar DK, Maitra A. Ketorolac entrapped in polymeric micelles: preparation, characterisation and ocular anti-inflammatory studies. *Int J Pharm*, 2000; 209(1-2): 1-14.2.
62. Foziyah Zakir, Singh Manvi, Iqbal Zeenat. Ocular drug delivery: Recent updates. *International Journal of Drug Regulatory Affairs*, 2016; 4(4): 15-22.
63. Marchal-Heussler L, et al: Antiglaucomatous activity of betaxolol chlorhydrates sorbed onto different isobutylcyanoacrylate nanoparticle preparations. *Int J Pharm*, 1990; 58: 115.
64. Giannavola, C et al: Influence of preparation conditions on acyclovir-loaded poly-D, L-lactic acid nanospheres and effect of PEG coating on ocular drug bioavailability. *Pharm Res*, 2003; 20: 584.
65. De campus AM, Diebold Y, Carvalho E, Sanchez A and Alonso MJ: chitosan nanoparticles as new ocular drug delivery systems: in vitro stability, in vivo fate, and cellular toxicity. *Pharmaceutical research*, 2004; 21: 803-810.
66. Barret ER. Nanosuspensions in drug delivery. *Nat Rev*, 2004; 3: 785-96.
67. James N. Chang. Recent advances in ophthalmic drug delivery. *Handbook of Non-Invasive Drug delivery system*. Elsevier, 2010; 165-192p.
68. Jagdale DM, Kamble VA and Kadam VJ: Nanosuspension a novel drug delivery system. *International Journal of Pharma and Bio Sciences*, 2017; 1(4): 352-60.
69. Patel, A, Cholkar, K, Agrahari, V. Ocular drug delivery systems: an overview. *World J Pharmacol*, 2013; 2(2): 47-64.
70. Kaur, IP, Garg, A, Singla, AK. Vesicular systems in ocular drug delivery: an overview. *Int J Pharm*, 2004; 269: 1-14.
71. Li, N, Zhuang, C, Wang, M. Liposome coated with low molecular weight chitosan and its potential use in ocular drug delivery. *Int J Pharm*, 2009; 379: 131-138.
72. Kaiser, JM, Imai, H, Haakenson, JK. Nanoliposomal minocycline for ocular drug delivery. *Nanomedicine*, 2013; 9: 130-140.
73. Seyfoddin, A, Al-Kassas, R. Development of solid lipid nanoparticles and nanostructured lipid carriers for improving ocular delivery of acyclovir. *Drug Dev Ind Pharm*, 2013; 39(4): 508-519.
74. Quintana, A, Raczka, E, Piehler, L. Design and function of a dendrimer-based therapeutic nanodevice targeted to tumor cells through the folate receptor. *Pharm Res*, 2002; 19(9): 1310-1316.
75. Padilla, De, Jesús, OL, Ihre, HR, Gagne, L. Polyester dendritic systems for drug delivery applications: in vitro and in vivo evaluation. *Bioconj Chem*, 2002; 13(3): 453-461.
76. Ihre, HR, Padilla, De, Jesús, OL, Szoka, FC. Polyester dendritic systems for drug delivery applications: design, synthesis, and characterization. *Bioconj Chem*, 2002; 13: 443-452.
77. Fischer, M, Vögtle, F. Dendrimers: from design to application—a progress report. *Angew Chem Int Ed*, 1999; 38: 884-905.
78. Abdelkader, H, Alany, RG. Controlled and continuous release ocular drug delivery systems: pros and cons. *Curr Drug Deliv*, 2012; 9: 421-430.
79. Gaudana, R, Jwala, J, Boddu, SHS. Recent perspectives in ocular drug delivery. *Pharm Res*, 2009; 26(5): 1197-1216.
80. Spataro, G, Malecaze, F, Turrin, CO. Designing dendrimers for ocular drug delivery. *Eur J Med Chem*, 2010; 45: 326-334.
81. Hao Chen, Yingying Jin, Lin Sun, Xi Li, Kaihui Nan, Huihua Lia. Recent development in ophthalmic drug delivery systems for therapy of both anterior and posterior segment diseases. *Colloid and Interface Science Communications*. Elsevier, 2018; 24: 54-61.
82. Jae Hwan Jung, Bryce Chiang, Hans E. Grossniklaus, Mark R Prausnitz. Ocular drug delivery targeted by Iontophoresis in the suprachoroidal space using Microneedle. *Journal of controlled release*. Elsevier. 2018; 277: 14-22.
83. Kurtis Moffatt, Yujing Wang, Thakur Raghu Raj Singh, Ryan F Donnelly. Microneedles for enhanced transdermal and intraocular drug delivery. *Current opinion Pharmacology*. Elsevier, 2017; 36: 14-21.
84. Gupta H, Aqil M. Contact lenses in ocular therapeutics. *Drug Discov Today*, 2012; 17(9-10): 522-527.
85. Bengani LC, Chauhan A. Extended delivery of an anionic drug by contact lens loaded with a cat-ionic surfactant. *Biomaterials*, 2013; 34(11): 2814-2821.
86. Kim J, Conway A, Chauhan A. Extended delivery of ophthalmic drugs by silicone hydrogel contact lenses. *Biomaterials*, 2008; 29(14): 2259-2269.
87. Prina Mehta, Ali Al-Kinani, Muhammad Sohail Arshad, Ming-Wei Chang, Raid G Alany. Development and Characterisation of electrospun timolol maleate-loaded polymeric contact lens coatings containing various permeation enhancers. *International Journal of Pharmaceutics*, 2017; 532(1): 408-420.
88. K. S. Rathore, R. K. Nema, S. S. Sisodia. An overview and advancement in ocular drug delivery systems. *International Journal of Pharmaceutical sciences and research*, 2010; 1(10): 11-23.
89. Karthikeyan D, Sonkar S, Pandey V.P, Nandha Kumar J, Sengottuvelu S, Bhowmick M, Shivakumar T. Development and Characterization of Modified Ocular Inserts with improved ocular compatibility. *Research Journal of Pharmacy and Technology*, 2008; 1(2): 93-9.